Multi-objective Optimization for Supporting Radiation Therapy Treatment Planning

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1 Radiotherapy Treatment Planning

- 2 Multi-objective Linear Programming
- 3 Visualising Trade-offs
- 4 Finite Representation of Non-dominated Sets
- 5 A Treatment Planning Session

Radiotherapy Treatment Planning Multi-objective Linear Programming

Visualising Trade-offs Finite Representation of Non-dominated Sets A Treatment Planning Session





1 Radiotherapy Treatment Planning

- 3 Visualising Trade-offs

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Radiotherapy Treatment Planning

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Radiotherapy



George sang along to the tune, wondering what the big deal was about Radiotherapy

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Radiotherapy Treatment Planning Multi-objective Linear Programming Visualising Trade-offs Finite Representation of Non-dominated Sets

A Treatment Planning Session

Radiotherapy

(Intensity Modulated Radiotherapy) IMRT represents an advance in the means that radiation is delivered to the target, and it is believed that IMRT offers an improvement over conventional and conformal radiation in its ability to provide higher dose irradiation of tumor mass, while exposing the surrounding normal tissue to less radiation.

http://www.cancernews.com/data/Article/259.asp





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Radiotherapy Treatment Planning

For each beam directions find a fluence map such that the resulting dose distribution achieves the treatment goals of tumour control and normal tissue protection





Radiotherapy Treatment Planning

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Mathematical Model



 a_{ij} = dose delivered to voxel *i* by unit intensity of bixel *j*

$$x_j = \text{intensity of bixer } j$$

 $d_i =$ dose delivered to

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voxel i

A Multi-objective Linear Programming Model

$$\begin{array}{rcl} \min & (\alpha, \beta, \gamma) \\ \text{s.t.} & TLB - \alpha e & \leq & A_{\mathcal{T}}x & \leq & TUB \\ & A_{\mathcal{C}}x & \leq & CUB + \beta e \\ & A_{\mathcal{N}}x & \leq & NUB + \gamma e \\ & 0 & \leq & \alpha & \leq & \alpha UB \\ & 0 & \leq & \alpha & \leq & \beta UB \\ & 0 & \leq & \gamma & \leq & \gamma UB \\ & 0 & \leq & x. \end{array}$$

- $\alpha UB, \beta UB, \gamma UB$ restrict solutions to clinically relevant values
- MOLP is always feasible and bounded
- Multi-objcetive version of elastic LP model of (Holder, 2003)

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- 2 Multi-objective Linear Programming
- 3 Visualising Trade-offs
- 4 Finite Representation of Non-dominated Sets
- 5 A Treatment Planning Session

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Multi-objective Linear Programming

$$\min\{Cx : Ax \ge b, x \in \mathbb{R}^n\}$$
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- $C \in \mathbb{R}^{p \times n}$, $A \in \mathbb{R}^{m \times n}$, $b \in \mathbb{R}^m$
- $X = \{x \in \mathbb{R}^n : Ax \ge b\}$
- $Y = \{Cx \in \mathbb{R}^p : x \in X\}, \mathcal{P} = Y + \mathbb{R}^p_{\geq}$
- x̂ ∈ X is (weakly) efficient if there is no x ∈ X with Cx ≤ Cx̂ (Cx < Cx̂)
- If \hat{x} is (weakly) efficient then $C\hat{x}$ is (weakly) non-dominated
- X_{wE} set of weakly efficient solutions, Y_{wN} set of non-dominated points
- $\hat{x} \in X$ is (weakly) ε -efficient if there is no $x \in X$ with $Cx \leq (\langle C \hat{x} \varepsilon \rangle$.
- $C\hat{x}$ is (weakly) ε -nondominated

An MOLP Example



Matthias Ehrgott, Lizhen Shao MOO for radiotherapy

Solution Methods

- Simplex methods: Exponential number of efficient extreme points
- Interior point methods: Find single solution or efficient facet
- Objective space methods: Smaller dimension

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Objective Space Algorithms

- Benson (1998), Ehrgott *et al.* (2012): Primal exact algorithm to compute P_{wN}
- Shao and Ehrgott (2008a): Primal approximation algorithm to compute set of weakly ε -nondominated points
- (Ehrgott *et al.*, 2012): Dual exact algorithm to compute \mathcal{P}_{wN}
- (Shao and Ehrgott, 2008b): Dual approximation algorithm to compute set of weakly ε-nondominated points

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Primal Exact Algorithm

$$\begin{aligned} &P_2(y) & \min\{z : Ax \geqq b, Cx - ez \leqq y\} \\ &D_2(y) & \max\{b^T u - y^T w : A^T u - C^T w = 0, e^T w = 1, u, w \geqq 0\} \end{aligned}$$

Algorithm

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An Outer Approximation Approach

- Find best values of all objectives
- Step 1: Connect extreme point with interior point, find intersection, and find supporting hyperplane
- Update corner points and repeat until no corner points outside feasible set left



An Outer Approximation Approach

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An Outer Approximation Approach

- Find best values of all objectives
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Primal Approximation Algorithm

- If $d(s^k, y^k) < \epsilon$ do not construct hyperplane
- Keep $s^k \in \mathcal{O}$ and $y^k \in \mathcal{I}$ for outer and inner approximation

•
$$V_o(\mathcal{S}^{k-1}) = \operatorname{vert}(\mathcal{S}^{k-1}), \ \mathcal{V}_i(\mathcal{S}^{k-1}) = (\operatorname{vert}(\mathcal{S}^{k-1}) \setminus \mathcal{O}) \cup \mathcal{I}$$

•
$$\mathcal{P}^i = \operatorname{conv}(\mathcal{V}_i(\mathcal{S}^{k-1})), \ \mathcal{P}^o = \operatorname{conv}(\mathcal{V}_o(\mathcal{S}^{\mathcal{K}}))$$

Theorem

Let $\varepsilon = \epsilon e$, where $e = (1, ..., 1) \in \mathbb{R}^{p}$. Then \mathcal{P}_{wN}^{i} is a set of weakly ε -nondominated points of \mathcal{P} .

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The Geometric Dual MOLP Heyde and Löhne (2008)

• Primal MOLP:

$$\min\{Cx: x \in \mathbb{R}^n, Ax \ge b\}$$

•
$$\mathcal{K} := \mathbb{R}_{\geq} e^{p} = \{ y \in \mathbb{R}^{p} : y_1 = \cdots = y_{p-1} = 0, y_p \geq 0 \}$$

• Dual MOLP:

 $\max_{\mathcal{K}} \{ D(u,\lambda) : (u,\lambda) \in \mathbb{R}^m \times \mathbb{R}^p, (u,\lambda) \geqq 0, A^T u = C^T \lambda, e^T \lambda = 1 \}$

$$D(u,\lambda) := (\lambda_1, ..., \lambda_{p-1}, b^T u)^T = \begin{pmatrix} 0 & I_{p-1} & 0 \\ b^T & 0 & 0 \end{pmatrix} \begin{pmatrix} u \\ \lambda \end{pmatrix}$$

• $\mathcal{D} := D(U) - \mathcal{K}$

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Let $(u, \lambda) \in U$ and $x \in X$ be feasible solutions to the dual and primal MOLP:

$b^T u = \lambda^T C x$

if and only if Cx is a weakly nondominated point of \mathcal{P} and $(\lambda_1, \ldots, \lambda_{p-1}, b^T u)$ is a \mathcal{K} -nondominated point of \mathcal{D} .

$$\varphi(y, \mathbf{v}) := \sum_{i=1}^{p-1} y_i \mathbf{v}_i + y_p \left(1 - \sum_{i=1}^{p-1} \mathbf{v}_i\right) - \mathbf{v}_p$$

Theorem (Heyde and Löhne (2008))

There is an inclusion reversing one-to-one map Ψ between the set of all proper \mathcal{K} -nondominated faces of \mathcal{D} and the set of all proper weakly nondominated faces of \mathcal{P} .

Moreover, for every proper \mathcal{K} -maximal face \mathcal{F}^* of \mathcal{D} and its associated proper \mathcal{K} -nondominated face $\Psi(\mathcal{F}^*)$ of \mathcal{P} it holds

 $\dim \mathcal{F}^* + \dim \Psi(\mathcal{F}^*) = p - 1$

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Dual Exact Algorithm

$$P_1(v) \quad \min \left\{ \lambda(v)^T C x : x \in \mathbb{R}^n, Ax \ge b \right\}$$
$$D_1(v) \quad \max \left\{ b^T u : u \in \mathbb{R}^m, u \ge 0, A^T u = C^T \lambda(v) \right\}$$
$$\lambda(v) = (v_1, \dots, v_{p-1}, 1 - \sum_{k=1}^{p-1} v_i)$$

Algorithm

Init:	Compute $\hat{d} \in int \mathcal{D}$ find optimal solution x^0 of $P_1(\hat{d})$				
	Set $\mathcal{S}^0 := \{ v \in \mathbb{R}^p : \lambda(v) \geqq 0, \varphi(Cx^0, v) \geqq 0 \}; k := 1$				
lt <i>k</i> 1 :	If $vert(\mathcal{S}^{k-1}) \subset \mathcal{D}$ STOP: $\mathcal{S}^{k-1} = \mathcal{D}$				
	<i>Otherwise choose</i> $s^k \in vert(\mathcal{S}^{k-1}) \setminus \mathcal{D}$				
lt k2 :	Find α^k with $v^k := lpha^k s^k + (1 - lpha^k) \hat{d} \in bd \mathcal{D}$				
It <i>k</i> 3 :	Compute optimal solution x^k of $P_1(v^k)$				
	Set $\mathcal{S}^k := \mathcal{S}^{k-1} \cap \{ v \in \mathbb{R}^p : \varphi(\mathcal{C}x^k, v) \geqq 0 \}$				

An Interior Approximation Approach



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Dual Approximation Algorithm

- If $\operatorname{vert}(\mathcal{S}^k) \subset \mathcal{D} + \epsilon e^p$ do not construct hyperplane
- If $v_p f \leq \epsilon$ then $v \in \mathcal{D} + \epsilon e^p$ where f is optimum of $D_2(v)$
- $\mathcal{D}^o := \mathcal{S}^{k-1} \supset \mathcal{D}$ is outer approximation of \mathcal{D}

$$\mathcal{P}^i:=\mathcal{D}(\mathcal{D}^o)\subset\mathcal{D}(\mathcal{D})=\mathcal{P}$$

is inner approximation of $\ensuremath{\mathcal{P}}$

Theorem

Let $\varepsilon = \epsilon e$, then \mathcal{P}_{wN}^i is a set of weakly ε -nondominated points of \mathcal{P} .

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- $\epsilon = 3/20$
- Two cuts as before
- $d(v^1, bd^1) = 1/8$, $d(v^2, bd^2) = 1/8$

•
$$\mathcal{D}^o = \mathcal{S}^2$$

•
$$\mathcal{P}^i = \mathcal{D}(\mathcal{D}^o)$$



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$$\epsilon = 3/20$$

- Two cuts as before
- $d(v^1, bd^1) = 1/8,$ $d(v^2, bd^2) = 1/8$
- $\mathcal{D}^o = \mathcal{S}^2$
- $\mathcal{P}^i = \mathcal{D}(\mathcal{D}^o)$





- 2 Multi-objective Linear Programming
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 - 4 Finite Representation of Non-dominated Sets
- 5 A Treatment Planning Session

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The Test Cases







Pancreatic Lesion

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Acoustic Neuroma Prostate

- Dose calculation inexact
- Inaccuracies during delivery
- Planning to small fraction of a Gy acceptable

Case	AN	Р	PL
Tumour voxels	9	22	67
Critical organ voxels	47	89	91
Normal tissue voxels	999	1182	986
Bixels	594	821	1140
TUB	87.55	90.64	90.64
TLB	82.45	85.36	85.36
CUB	60/45	60/45	60/45
NUB	0.00	0.00	0.00
αUB	16.49	42.68	17.07
βUB	12.00	30.00	12.00
γUB	87.55	100.64	90.64

	ϵ	Solving the dual			Solving the primal
		Time	Vert.	Cuts	Time Vert. Cuts
AC	0.1	1.484	17	8	5.938 27 21
	0.01	3.078	33	18	8.703 47 44
	0	8.864	85	55	13.984 55 85
PR	0.1	4.422	39	19	14.781 56 42
	0.01	18.454	157	78	64.954 296 184
	0	792.390	3280	3165	995.050 3165 3280
PL	0.1	58.263	85	44	164.360 152 90
	0.01	401.934	582	298	1184.950 1097 586
	0.005	734.784	1058	539	2147.530 1989 1041

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- 2 Multi-objective Linear Programming
- 3 Visualising Trade-offs
- 4 Finite Representation of Non-dominated Sets
- 5 A Treatment Planning Session

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Finite Representation

Definition

A finite representation of Y_N is a subset R of Y_N such that $|R| < \infty$.

Criteria for quality of representation (Sayin, 2000)

- Cardinality contains reasonable number of points
- Q Uniformity does not contain points that are very close to each other
 Uniformity level δ := min_{r¹,r²∈R} d(r¹, r²)
- Coverage contains point close to each nondominated point Coverage error ε := max_{y∈YN} min_{r∈R} d(y, r)

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Finite Representation

Definition

Let R be a representation of Y_N , d a metric and $\varepsilon > 0$ and $\delta > 0$ be real numbers.

- *R* is called a d_{ε} -representation of Y_N if for any $y \in Y_N$, there exists $r \in R$ such that $d(y, r) \leq \varepsilon$.
- *R* is called a δ-uniform d_ε-representation if min<sub>r¹,r²∈R,r¹≠r²{d(r¹, r²)} ≥ δ.
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Existing Methods



Global shooting method (Benson and Sayin, 1997) Good coverage Uniformity can be bad

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Existing Methods



Normal boundary intersection (NBI) method (Das and Dennis, 1998) Good uniformity Coverage may be bad

The Revised Boundary Intersection Method



Input: MOLP data A, b, C and ds > 0.

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The Revised Boundary Intersection Method



Find
$$y^{AI}$$
 defined by
 $y_k^{AI} = \max\{y_k : y \in Y\},\ k = 1, \dots, p.$

Image: A math a math

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Matthias Ehrgott, Lizhen Shao MOO for radiotherapy

The Revised Boundary Intersection Method



Find a non-dominated point \hat{y} by solving the LP $\phi := \min\{e^T y : y \in Y\}.$

The Revised Boundary Intersection Method



Compute p + 1 points $v^k, k = 0, ..., p$ in \mathbb{R}^p $v^k = \int y_l^{Al}, \qquad l \neq k$

$$\mathbf{v}_l^k = \begin{cases} \mathbf{y}_l^m, & l \neq k, \\ \phi + \hat{\mathbf{y}}_k - \mathbf{e}^T \mathbf{v}^0 & l = k. \end{cases}$$

The convex hull S of $\{v^0, \ldots, v^p\}$ is a simplex containing Y. The convex hull \hat{S} of $\{v^1, \ldots, v^p\}$ is a hyperplane with normal e supporting Y in \hat{y} .

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The Revised Boundary Intersection Method



Compute equally spaced reference points q^i with distance ds on \hat{S} .

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The Revised Boundary Intersection Method



For each reference point qsolve the LP min{ $t : q + te \in Y, t \ge 0$ }. If this LP is infeasible, the ray q + te does not intersect Y, otherwise for the optimal value $\hat{t}, q = \hat{t}y \in Y$. The LP cannot be unbounded.

The Revised Boundary Intersection Method



For each weakly non-dominated point \hat{y} found in the previous step solve the LP $\min\{e^T y : y \in Y, y \leq \hat{y}\}$. It holds that \hat{y} is non-dominated if and only if it is an optimal solution of this LP.

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The Revised Boundary Intersection Method



Output: Representation *R* consisting of the non-dominated points confirmed in the last step.

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Revised Normal Boundary Intersection

Theorem

Let R be the representation of Y_N obtained with the RNBI method and let q^1, q^2 be two reference points with $d(q^1, q^2) = ds$ that yield non-dominated representative points r^1, r^2 . Then $ds \leq d(r^1, r^2) \leq \sqrt{p} ds$. Hence R is a ds-uniform representation of Y_N .

Theorem

Let R be the representation of Y_N obtained with the RNBI method and assume that the width $w(S^j) \ge ds$ for the projection S^j of all maximal faces Y^j of Y_N on \hat{S} . Then R is a ds-uniform $d_{\sqrt{p}ds}$ -representation of Y_N .

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- 2 Multi-objective Linear Programming
- 3 Visualising Trade-offs
- 4 Finite Representation of Non-dominated Sets
- 5 A Treatment Planning Session

- 4 同 ト - 4 三 ト - 4

Acoustic Neuroma



- 3 CT images, 3mm voxel size
- 78 tumour voxels, 472 critical organ voxels, 6778 normal tissue voxels, 597 bixels
- TLB = 57.58, TUB = 61.14, CUB(brain stem) = 50, CUB(eyes) =5 Gy, NUB = 0

MOLP size

$$m = 7.410, n = 600, p = 3$$

Acoustic Neuroma



- ds = 3.47 (153 reference points)
- 22 nondominated points (140 seconds of CPU time)
- Points marked are referred to in the simulated planning session

Finding a Suitable Plan



Plan 1, objectives as equal as possible (3.882, 2.366, 36.354)

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Finding a Suitable Plan



Plan 2, objective values (2.663, 6.048, 37.585) depicted by +

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Finding a Suitable Plan



Plan 3, objective values (5.231, -1.185, 35.253) depicted by \diamond

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Finding a Suitable Plan



Plan 4, objective values (2.770, -1.196, 37.693) depicted by ⊡

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Finding a Suitable Plan



Plan 5, objective values (5.148, 6.083, 35.170) depicted by \triangleright

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